Simultaneous multi-slice excitation in spatial encoded NMR experiments



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Introduction

Recently, it has appeared a growing interest in spatially localized NMR spectroscopic techniques. Several high-resolution NMR methods applying spatial frequency encoded excitation into the NMR tube have been proposed for obtaining specific information from a particular slice as, for instance, to obtain broadband homodecoupled ¹H spectra using the Zangger-Sterk (ZS) method¹.

The most serious drawback of spatially encoded NMR experiments is their reduced sensitivity because the observed signal only arises from a discrete slice of the sample. In this work, we exploit the sensitivity benefits of applying a multiple-frequency modulated pulse to excite simultaneously different slices in a single NMR experiment. Our proposal is based on the careful setting of multiple offsets to avoid the excitation of mutually J-coupled protons into the same slice which would produce distorted multiplets due to J_{HH} evolution².



Methodology



Figure 1: Pulse sequences of the A) 1D z-profile image, B) 1D spatially-encoded single pulsed-field gradient echo (se-SPFGE) and C) ¹H pure-shift experiments. Spatial frequency encoding is achieved by simultaneous application of a spatial-encoding gradient (G_s) and a frequency-selective 180^o ¹H pulse. The G_s gradient is adjusted to cover a spectral width of k*SW_{1H} (k≥1). G_1 gradients act as defocusing/refocusing coherence elements. The duration of G_3 gradient is two times G_2 . The delays τ_a , τ_b and τ_c are automatically calculated so that $\tau_a + \tau_c = \tau_b$; $\tau_a = \tau_c$; $\tau_a = 1/4$ *SW₁.

Experimental Part

Evaluation of effectiveness of multiple-frequency pulses

We have used two basic experiments (Fig. 1A-B) to evaluate the effectiveness of multiplefrequency pulses in slice-selective spectra: 1D z-profile image (Fig. 2A-F) and se-SPFGE experiments (Fig. 2G-L) to visualize the frequency excitation achieved along the z dimension and the experimental effects on the NMR spectrum, respectively.



Application of multiple-frequency pulses

As a proof of the method, we have applied it on a sample of ibuprofen, that contains a relative simple ¹H spectrum (Fig. 3A), and on a sample of cyclosporine, which presents a more complex ¹H spectrum (Fig. 4A).





Figure 2: A-F) Schematic z-profile of a 99.96% D_2O sample (pulse sequence used shown in Fig. 1A) using a multiple-frequency pulse with 0 (G_s =off), 1, 2, 4, 8 and 16 different offsets, respectively; G-L) se-SPFGE spectra (pulse sequence used shown in Fig. 1B) using a multiple-frequency pulse with 1, 2, 4, 8 and 16 different offsets and with the experimental signal-to-noise ratio related to the conventional ¹H NMR spectra (I). In all experiments, a 20ms Gaussian-shaped 180^o ¹H pulse was simultaneous applied with an encoding gradient of 0,865 G/cm.

Conclusions

 \checkmark The simultaneous multi-slice excitation improves the sensitivity of slice-

Figure 3: A) Conventional ¹H NMR spectra of ibuprofen in $CDCl_3$. The experimental S/N ratio has been normalized for each individual signal. B) Signals arising of individual SPFGE experiments (G_s =0) to account for T_2 relaxation losses during the echo. C,D) single-slice se-SPFGE spectra using a normalized scaling k factor of 1 and 2, respectively. E) Multi-slice se-SPFGE spectrum using an amplification k factor of 2 and 15 different offsets. A single scan and a 20ms Gaussian-shaped pulse were used in all experiments. Spectrum C was recorded using a square-shaped encoding gradient of 0.495 G/cm and spectra D and E with a G_s of 0.99 G/cm.



Figure 4: A) Conventional ¹H NMR spectra of cyclosporine in benzene-d6. The experimental S/N ratio has been normalized for each individual signal. B) Signals arising of individual SPFGE experiments (G_s =0). C,D) single-slice se-SPFGE spectra using normalized scaling k factor of 1 and 2 respectively. E) Multi-slice se-SPFGE spectrum using an amplification k factor of 2 and 22 different offsets. A single scan and a 20ms Gaussian-shaped pulse were used in all experiments. Spectrum C was recorded using a square-shaped encoding gradient of 0.59 G/cm and spectra D and E with a G_s of 1.196 G/cm.

Broadband homodecoupled ¹H experiments using the pure-shift pseudo-2D technique²



selective NMR experiments.

The experimental effects on the NMR spectrum can be quickly monitored by recording se-SPFGE experiments.

Easy implementation without need to modify existing pulse sequences, so can be immediately adapted to a wide range of applications.

References

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Figure 5: Sensitivity-enhanced broadband-homodecoupled ¹H NMR spectra of ibuprofen. A) Conventional ¹H spectrum; B) and C) show the single-slice and 8-site multi-slice pure-shift experiment, respectively. An amplification k factor of 2, a square-shaped G_s of 0.99 G cm⁻¹ and a 20ms Gaussian-shaped 180° ¹H pulse were used in all experiments. 8 transients were collected for each one of the 32 t₁ increments of 0.68 s each were acquired with $1/SW_1$ = 10ms and a relaxation delay of 1 s, in total time of 8 min.

Figure 6: Sensitivity-enhanced broadband-homodecoupled ¹H NMR spectra of cyclosporine. Expanded H_{α} region from the A) conventional; B,C) single-slice and 8-site multi-slice pure-shift ¹H spectra, respectively. An amplification k factor of 2, a square-shaped G_s of 1.13 G/cm and a 80 ms Rsnob 180^o ¹H pulse were used in all experiments. 4 transients were collected for each one of the 32 t₁ of 0.68 s each were acquired with 1/SW₁= 10ms and a relaxation delay of 1 s, in total time of 4 min.

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